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PICTORIAL REVIEW

Utility of double inversion recovery MRI in paediatric epilepsy

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ABSTRACT

Detecting focal abnormalities in MRI examinations of children with epilepsy can be a challenging task given the frequently subtle appearance of cortical dysplasia, mesial temporal sclerosis and similar lesions. In this report, we demonstrate the utility of double inversion recovery MRI in the detection of paediatric epileptogenic abnormalities, promoted primarily by increased lesion conspicuity due to complementary suppression of both cerebrospinal abnormalities and normal white matter signal.

INTRODUCTION

Identifying structural abnormalities that correspond to an epileptogenic focus is frequently a challenging task with the available MRI imaging techniques. Advances in spatial and contrast resolution have made possible the detection of subtle findings in patients with epilepsy, particularly focal cortical dysplasia (FCD) in paediatric patients. Given the cortical location of these lesions and the associated blurring of the underlying white matter, an MRI sequence that highlights cortical and subcortical pathology and increases the conspicuity of abnormal white matter is naturally a suitable candidate to be successfully employed in this clinical scenario.

Double inversion recovery (DIR) MRI has been proposed in central nervous system imaging, given its improved lesion-to-background contrast driven by simultaneous suppression of signal from both cerebrospinal fluid and normal white matter. The technique involves application of two inversion recovery pulses. The timing of the pulses is set so that the longitudinal magnetization from cerebrospinal fluid (CSF) and from white matter passes simultaneously through the null point. Image acquisition then proceeds with a standard fast spin echo sequence that samples the remaining magnetization, which is predominantly from grey matter.

DIR has been previously applied in the evaluation of multiple sclerosis and demonstrated increased sensitivity for depiction of cortical lesions, both at 1.5 T and at 3.0 T. Utilizing quantitative analysis of signal intensities, DIR has also proved beneficial in characterizing epileptogenic foci related to congenital and acquired neocortical pathology. In temporal lobe epilepsy, DIR has demonstrated superior sensitivity compared with $T_2$ fluid-attenuated inversion-recovery and strong agreement with positron emission tomography for localization of epileptogenic focus. It has also proved valuable in the identification of cortical tubers in patients with tuberous sclerosis.

The aim of this report is to illustrate the advantages and pitfalls of DIR imaging in patients with epilepsy, highlighting the increased conspicuity for detection of subtle congenital and acquired abnormalities.

CASE SERIES

Using data aggregation and search technology software for our institution’s picture archiving and communication system/radiology information system, several illustrative cases of the diagnostic value and pitfalls of DIR were identified. This study was approved by the institutional review board.
The DIR implementation currently employed at our institution consists of a coronal 3D acquisition of the whole head utilizing body transmit and local signal reception with dedicated 32-channel head coil. All imaging was performed on a 3.0-T clinical whole-body system (Siemens Tim Trio; Figure 1).

**IMAGE ACQUISITION**

Figure 1. Normal perirolandic cortex. Axial $T_1$ weighted three-dimensional magnetization prepared rapid gradient echo (a) and reformatted double inversion recovery (DIR) (b) images. $T_1$ weighted image shows very subtle high signal intensity in the perirolandic cortex with respect to the remainder of the cortex. On the DIR image, the perirolandic cortex appears relatively low in signal intensity (arrows).

Figure 2. Normal hippocampus. Coronal $T_2$ weighted (a), $T_2$ fluid-attenuated inversion-recovery (b) and double inversion recovery (c) images. The normal hippocampi are slightly brighter than the normal supratentorial neocortex on $T_2$ weighted sequences, owing to different cytoarchitecture.
Siemens Medical Solutions, Erlangen, Germany), with the DIR sequences acquired as a modification to a 3D $T_2$ weighted acquisition (sampling perfection with application optimized contrasts using different flip angle evolution) permitting for flexibility in k-space sampling strategy, echo trains and flip angle evolution schemes, as well as two

Figure 3. Incomplete myelination in a 20-month-old child. Sagittal reformatted double inversion recovery (DIR) (a) and sagittal $T_2$ fluid-attenuated inversion-recovery (b) images show relatively increased signal intensity in the white matter of the anterior temporal lobes when compared with the frontal white matter. This difference, due to incomplete myelination, is most conspicuous on the DIR image (arrows). Despite the apparent blurring of the grey-white matter junction, this is a normal finding when symmetric.

Figure 4. Mesial temporal sclerosis. Coronal $T_2$ weighted (a), $T_2$ fluid-attenuated inversion-recovery (b) and double inversion recovery (DIR) (c) images. The left hippocampus is atrophic and hyperintense (arrow in c). Asymmetry of signal intensity of the hippocampi is most conspicuous on the DIR image. However, the normal internal architecture of the right hippocampus is better depicted on the $T_2$ weighted image (arrow in a).
separate inversion times in a DIR operation block. Contrast optimization is achieved through simulation parameters provided inline, together with the spatially non-selective double-inversion preparation for suppression of both CSF and white matter. Sequence parameters for fat-suppressed coronal 3D DIR were prescribed as follows: TR 7500 ms; TE 327 ms; T11 3000 ms; T12 450 ms; excitations 1; voxel size 1-mm isotropic; turbo factor 256; BW 789 Hz/pixel; field of view 200 × 173 mm; parallel acceleration factor (iPAT) 2; acquisition time 7 min 24 s. Note that some of the cases presented in this essay were acquired using an eight-channel head coil and show a relatively lower spatial resolution when compared with our present technique.

NORMAL ANATOMY
The normal perirolandic cortex appears thinner and less well-defined than the remainder of the neocortex on DIR imaging (Figure 1), owing to cytoarchitectural differences including increased myelination. In addition, the normal hippocampi and amygdala are slightly hyperintense than the supratentorial neocortex on DIR sequences and on other T2 weighted sequences (Figure 2).

Normal areas of evolving myelination are conspicuous on DIR imaging, appearing as areas of brighter signal when compared with fully myelinated white matter. This is due to relatively diminished T2 shortening of the unmyelinated white matter.

Figure 5. Ictal changes. Coronal T2 weighted (a), T2 fluid-attenuated inversion-recovery (b) and double inversion recovery (DIR) (c) images. The left hippocampus is swollen and hyperintense but retains its normal internal architecture on the T2 weighted image. Asymmetry of signal intensity of the hippocampi is most conspicuous on the DIR image (arrow).
MESIAL TEMPORAL SCLEROSIS
Although relatively less common in children than in adults suffering from refractory epilepsy,16 mesial temporal sclerosis nevertheless represents a diagnostic challenge on MRI when the findings of hippocampal atrophy, T₂ hyperintense signal and disruption of internal architecture are subtle, such as in the early stage. DIR imaging is beneficial by demonstrating increased conspicuity of asymmetric signal intensity of the hippocampi (Figure 4). However, the internal architecture of the hippocampus is better depicted on T₂ weighted imaging.

Recent seizures may cause swelling and T₂ hyperintense signal in the affected hippocampus. In this setting, DIR imaging conspicuously demonstrates the asymmetric signal hyperintensity of the hippocampi (Figure 5).
FOCAL CORTICAL DYSPLASIA AND TUBEROUS SCLEROSIS
FCD, particularly the Type IIb, and cortical tubers are commonly associated with radial glial abnormality extending to the wall of the lateral ventricle (also known as the transmantle sign). DIR imaging is excellent in depicting the transmantle sign and the boundaries of the white matter signal abnormality (Figures 6 and 7). It also depicts subtle Type I FCDs that are sometimes located in the temporal pole and characterized by incomplete asymmetric myelination of the subcortical white matter.

PERIVENTRICULAR NODULAR HETEROTOPIA
The suppression of normal white matter signal achieved with DIR imaging results in increased conspicuity of small foci of heterotopic grey matter (Figure 8). DIR may also help distinguish nodular heterotopia from small foci of gliosis, since the latter are typically brighter than normal grey matter.

POLYMICROGYRIA
Not all malformations of cortical development present with abnormal signal intensity on DIR imaging. Polymicrogyria occurs in later stages of cortical development (late migration/early organization); therefore, the abnormal cortex is relatively less dysplastic and may not exhibit the high signal intensity typically seen in FCD on T2 weighted images. Volumetric T1 weighted sequences also demonstrate similar signal intensity between normal cortex and areas of polymicrogyria (Figure 9).

NEUROGLIAL TUMOURS
DIR imaging provides high contrast between tumour and adjacent normal-appearing cortex (Figure 10). This facilitates the delineation of the extent of abnormal tissue prior to surgery for refractory epilepsy, particularly since neuroglial tumours may be associated with areas of cortical dysplasia that may contribute to epileptogenesis.18

DISCUSSION
Detection of focal pathology in MRI of children with intractable epilepsy aids pre-surgical planning and intraoperative management. However, abnormalities such as FCD are often subtle, justifying the effort in developing MR sequences that provide optimal contrast between normal and abnormal tissue. For example, Kadom et al reported on the utility of T1 weighted magnetization transfer images to detect FCDs in infants and young children with incomplete myelination. Chan et al reported accurate diagnosis and localization of FCD utilizing high-resolution T2 weighted fast multiplaner inversion recovery images. Excellent contrast between grey and white matter can also be achieved with DIR, consisting of two inversion pulses applied to simultaneously suppress the signal from two tissues with different longitudinal relaxation times. By selectively suppressing CSF and normal white matter signals, grey matter-only images can be obtained. Recent developments allow DIR to be performed utilizing multichannel coils at higher magnetic fields, providing high-resolution isotropic MR images.

DIR imaging has a potential beneficial role in lesion detection and lateralization in patients with epilepsy. We illustrate the role of DIR imaging in epilepsy in such cases as malformations of cortical development, mesial temporal sclerosis and neoplasms. In evaluating such cases, it is important to remain aware that differences in cytoarchitecture cause inherently higher signal intensities of the hippocampi (and to a lesser extent of the insular cortices) with DIR. Distinguishing the boundaries of an infiltrative tumour or cortical dysplasia from adjacent normal cortex or white matter is facilitated by DIR. Furthermore, given the increased conspicuity for identification of cortical tubers, DIR can be employed to subjectively quantify the burden of disease in tuberous sclerosis. However, despite the aforementioned advantages of DIR imaging, its diagnostic value is limited in the incompletely myelinated brain, where suppression of the MR signal from normal white matter relies on its narrow range of T1 values. Optimizing the inversion time for suppression of the normal unmyelinated white matter at different stages of brain development is an area of ongoing attention. In temporal lobe epilepsy, DIR was the most sensitive sequence for detection of unilateral abnormal
Figure 9. Polymicrogyria. Coronal $T_1$ weighted three-dimensional magnetization prepared rapid gradient echo (a), $T_2$ fluid-attenuated inversion-recovery (b) and double inversion recovery (DIR) (c) images. An area of abnormal gyral pattern with irregular contours is present in the right temporal lobe (arrows), consistent with polymicrogyria. On all images, including DIR, there is no appreciable difference in the signal intensity of the normal and abnormal cortex. Note also mild atrophy of the ipsilateral hippocampus, without associated signal abnormality. Adjacent areas of subcortical heterotopia were also present (not shown).

CONCLUSION

Given the increased conspicuity in the depiction of subtle abnormalities, we suggest acquisition of DIR imaging when imaging children with refractory epilepsy. Further studies are required to quantify the increased diagnostic accuracy provided by the DIR technique relative to conventional MRI sequences.
Figure 10. Dysembryoplastic neuroepithelial tumour. Axial T2 fluid-attenuated inversion-recovery (a) and reformatted axial double inversion recovery (DIR) (b) images of an intra-axial mass in the right frontal lobe with peripheral cystic components remodelling the inner table of the calvarium indicating slow growth. DIR provides precise delineation between tumour and adjacent normal-appearing cortex.

(a)  
(b)  

REFERENCES


